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# Mid-term comparison of highly porous versus hydroxyapatite-coated porous surface in the same cup system: a retrospective single-center study

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## Abstract

**Background** In this study, we aimed to compare the mid-term clinical and radiographic outcomes of highly porous and hydroxyapatite (HA)-coated porous titanium cups using the same cementless cup system in patients undergoing total hip arthroplasty (THA). We investigated the differences in radiolucent line (RLL) formation, cup migration, and clinical outcomes between the two surface processing methods.

**Methods** This retrospective study included 209 hips (116 in the highly porous group and 93 in the HA porous group) with a minimum follow-up period of over 4 years. Using standardized anteroposterior pelvic radiographs, we conducted radiographic evaluations to assess cup orientation, initial gaps, and RLLs. Migration was analyzed using Einzel-Bild-Röntgen Analysis (EBRA), focusing on a subset of 28 randomly selected cups from each group as determined by power analysis. Clinical outcomes were measured using the Japanese Orthopedic Association (JOA) hip score. The primary outcome was the incidence of cup revision, and the secondary outcomes were postoperative JOA scores and the incidence of initial gaps and RLLs.

**Results** No cup revisions were made in either group. Both groups had significant postoperative improvements in the JOA scores, with no differences observed during the follow-up period. At baseline, the initial gaps were observed at similar rates (highly porous vs. HA porous [51% vs. 52%];  $p=0.97$ ). However, at the 5-year follow-up, the initial gaps were resolved in nearly all cases. In the highly porous group, RLLs were significantly more frequent during the first-year follow-up (23% vs. 2%;  $p<0.0001$ ). However, they decreased in all cases, and none of them exhibited RLL expansion. EBRA migration analysis revealed no significant differences between the groups.

**Conclusion** Both groups demonstrated comparable mid-term clinical and radiographic outcomes. The highly porous group exhibited higher initial RLL incidences. However, RLL diminished over time without compromising the migration or clinical results. Both designs are reliable options for cementless THA.

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**Keywords** Highly porous titanium cups, Cementless cup system, Mid-term outcomes, Bone ingrowth, Hydroxyapatite-coated porous cups, Cup migration, Clinical outcomes, Three-dimensional-printed porous design

## Background

Total hip arthroplasty (THA) is an excellent treatment option for patients with severe hip joint disorders in terms of cost-effectiveness and significant clinical improvement [1]. The survival rates of long-term implants have exceeded 90% over the last 10 years [2]. However, early implant failure due to aseptic loosening remains a significant concern [3], necessitating revision surgeries, which affect patient-reported outcomes negatively [4]. Aseptic loosening of the acetabular cups due to poor initial fixation and insufficient bone ingrowth is critical for long-term implant success [5]. Therefore, improving implant longevity remains a critical issue in orthopedic surgery.

Historically, the evolution of the surface design and processing in cementless THA played a critical role in the survival rates of long-term implant survival, particularly for acetabular cups [6]. In cementless cups, conventional porous coatings such as porous plasma spray (PPS) processing with or without hydroxyapatite (HA) coating have demonstrated excellent clinical outcomes and durability for over 10 years [7, 8]. Recently, the three-dimensional (3D) highly porous processing, designed to mimic the trabecular structure of cancellous bone, was developed using advanced manufacturing techniques such as 3D printing technology. These highly porous structures are hypothesized to enhance bone ingrowth and provide superior initial stability based on biomechanical and osteogenic studies using animal models [9, 10]. However, reports of an early postoperative radiolucent line (RLL) and aseptic loosening in some cases have raised concerns regarding the effectiveness of highly porous coatings [11]. Comparisons of the clinical and radiographic outcomes between conventional porous coatings and newer highly porous coatings remain unclear.

Therefore, we aimed to elucidate the impact of different surface processing techniques within the same cup system by comparing the postoperative clinical and radiographic outcomes of the conventional HA porous with the highly porous coatings in the mid-term period. We hypothesized that the highly porous cups would demonstrate clinical and radiographic outcomes equivalent to those of HA-porous cups. From this comparison, we aim to provide a clearer understanding of the benefits and potential drawbacks of highly porous surface processing in cementless cups.

## Methods

In this retrospective cohort study, we analyzed 163 consecutive patients (214 hips) who underwent primary THA with G7 acetabular cup system (Zimmer Biomet, Warsaw, IN, USA) at the Institute of Science, Tokyo Hospital, between March 2014 and January 2017. Our institutional review board approved this study. We excluded patients with <4 years of follow-up or those with insufficient imaging evaluations. Based on the exclusion criteria, 14 patients were excluded; 13 (14 hips) were due to insufficient follow-up, and 1 patient (2 hips) was due to insufficient imaging. We enrolled 149 patients (198 hips). Patients were divided into two groups based on the G7 cup surface processing: G7 OsseoTi highly porous titanium cup (highly porous group; 109 hips) and G7 PPS BoneMaster cup coated HA (HA porous group; 89 hips). *The G7 OsseoTi surface employed CT-based 3D printing to mimic the human cancellous bone structure. This surface was manufactured using a proprietary layer-by-layer printing process to achieve a mean pore size of 475 microns and 70% porosity. The G7 PPS BoneMaster surface was produced using PPS titanium coating with a thin layer of hydroxyapatite.* The cup selection gradually shifted from HA porous cups to highly porous cups as the latter became available. In all cases, the type of stem used in this series was Taperloc Complete Microplasty Stem (Zimmer Biomet, Warsaw, IN, USA), except for one case in which a changeable neck stem with M/L Taper and Kinectiv Stem (Zimmer Biomet, Warsaw, IN, USA) were used due to anteversion adjustment. Four high-volume expert arthroplasty surgeons performed all surgeries. The acetabulum was under-reamed by 1 mm, and all the cementless cups were inserted using the press-fit technique in both groups. Adjunctive one or two screw fixation was performed at the surgeon's discretion. A highly cross-linked polyethylene liner and ceramic head were used in all cases. The target cup angles were set at 40° in radiographic inclination and 15°–20° in radiographic anteversion. Demographic data, including age, sex, body mass index (BMI), and underlying hip pathology, were collected from medical records. Surgical details such as approach, cup size, the number of screws, and cup revision surgery used were documented. Clinical outcomes were assessed using the Japanese Orthopedic Association (JOA) hip score (maximum 100 points); a high JOA score was indicative of better hip function [12]. Data was collected preoperatively and postoperatively at 1 year, 2–3 years (recorded as 2-year postoperative data), and 4–6 years (recorded as 5-year postoperative data).

### Radiographic analysis

Radiographic evaluations were conducted at baseline (within 1 week postoperatively) and at regular postoperative intervals: 1 year, 2–3 years (recorded as 2-year postoperative data), and 4–6 years (recorded as 5-year postoperative data). All anteroposterior (AP) pelvic radiographs were obtained in a standardized manner (patient standing in an upright position and full weight-bearing) [13]. AP pelvic radiographs were analyzed to measure the cup inclination and anteversion angle and the presence of the initial gap and RLLs. The cup inclination angle was determined by measuring the angle between the inter-teardrop line and the major oblique axis of the cup. The cup anteversion angle was measured on AP pelvic radiographs using the method described by Lewinnek et al. [14]. The locations of the initial gap and RLL were classified using the acetabular zones proposed by DeLee and Charnley. The initial gap was defined as a gap of  $\geq 0.5$  mm between the cup and the acetabular host bone that could be detected on the postoperative radiographs within 1 week postoperatively. RLL was defined as radiolucency  $\geq 0.5$  mm without an initial gap [15]. Reliability assessments were conducted to detect the initial gap and RLL. Two independent orthopedic surgeons (TT and YT) not involved in the THA surgery tested inter and intra-observer agreements using a subset of 20 randomly selected hips, with measurements repeated at least 4 weeks apart. The inter-observer agreement rates for detecting the initial gaps and RLLs were 93% and 97%, respectively, and the intra-observer agreement rates were 99% and 99%, respectively. Using the McNemar test, no significant differences were observed in detection rates between inter- and intra-observer agreements for initial gaps ( $p=0.32$ ,  $p=1.0$ , respectively) or RLLs ( $p=0.56$ ,  $p=0.32$ , respectively), indicating equivalent detection reliability.

### Migration analysis with einzel-bild-röntgen analysis

Cup migration was analyzed using Einzel-Bild-Röntgen Analysis (EBRA) software (German: Einzel-Bild-Röntgen-Analyse), a validated method for assessing implant migration without markers [13]. A power analysis was conducted before the migration analysis to ensure statistical robustness. Based on the preliminary measurement, a standard deviation of 1.3 mm, and a clinically meaningful difference of 1.0 mm [13, 16], a sample size of 28 hips per group was required to achieve 80% power, with a significance level of 0.05. For migration analysis, 28 cups were randomly selected from both groups to assess potential differences in migration between the two groups. Migration was assessed as the total displacement vector calculated with the Pythagorean Theorem, and a clinically significant threshold of total migration was defined as  $\geq 2$  mm within the first 2 years [16].

### Statistical analysis

Statistical analyses were performed using the STATA 16 software (StataCorp LP, College Station, TX, USA). All continuous data are presented as means  $\pm$  standard deviations (SD). We performed the Shapiro–Wilk test to assess the normality of the data. For continuous parameters with a normal distribution, we used the unpaired t-test for statistical comparisons. For non-normally distributed data, we applied the non-parametric Mann–Whitney U test. Chi-square analyses were used to assess the associations between discrete variables (the presence of initial gaps and RLLs). The significance level was set at  $p < 0.05$  for all tests.

### Results

The highly porous and HA porous groups had comparable demographic and clinical characteristics except for the follow-up period and head diameter (Table 1). The mean age, BMI, cup diameter, number of fixation screws, cup alignment, and surgery time were similar between the two groups. Both groups showed balanced distributions of sex, THA diagnosis, operation site, and surgical approach. The slight difference in the follow-up periods was due to the timing of availability of each cup. The head diameter was slightly smaller in the HA porous group.

During the observation period, no cup revision occurred in either group. Both groups demonstrated significant improvements in the JOA scores postoperatively, with no significant differences observed at any follow-up interval (Table 2). The preoperative scores were comparable, and the postoperative scores exceeded 90 points in both groups, reflecting excellent clinical outcomes.

The initial gaps were observed at comparable rates in both groups, and no significant differences were observed during the entire follow-up period (Table 3). At baseline, initial gaps were present in  $>50\%$  of the cases in both groups; however, at the 5-year follow-up, the incidence decreased to approximately 1% in both groups. At all postoperative intervals, RLLs were significantly more frequent in the highly porous group than in the HA group (Fig. 1). However, the incidence of RLLs decreased over time in both groups. Furthermore, in all cases with RLLs, there was no progressive widening of the RLLs or expansion of the affected zones over time (Table 4). Migration analysis using EBRA revealed no significant differences in the total migration between both groups at any follow-up period (Table 5). In addition, both groups exhibited stable migration patterns, with no cases exceeding the clinical threshold of 2 mm within the first 2 years.

### Discussion

In this study, we highlight the clinical and radiological outcomes of cementless THA performed with highly porous cups, compared with conventional HA-coated

**Table 1** Patients' demographic and clinical characteristics

Patient characteristics	Highly porous group (n = 109)	HA porous group (n = 89)	p-value
Age (years) <sup>*†</sup>	63.0 ± 10.8	62.4 ± 13.0	0.63
Sex, female/male <sup>‡</sup>	89/20	76/13	0.48
Body mass index (kg/m <sup>2</sup> ) <sup>*†</sup>	24.2 ± 3.8	23.3 ± 3.5	0.18
Diagnosis <sup>‡</sup>			
Primary hip osteoarthritis, n (%)	9 (8)	4 (4)	0.46
Secondary osteoarthritis due to dysplasia, n (%)	95 (87)	76 (86)	
Osteonecrosis of the femoral head, n (%)	5 (5)	9 (10)	
Operation side, R/L <sup>‡</sup>	56/53	44/45	0.79
Follow-up period (years) <sup>**†</sup>	5.7 ± 0.8 (3.7–6.9)	6.2 ± 0.8 (3.8–6.9)	<b>&lt; 0.001</b>
Surgical approach <sup>‡</sup>			
Anterolateral, n (%)	11 (10)	16 (18)	0.11
Posterolateral, n (%)	98 (90)	73 (82)	
Cup diameter (mm) <sup>*†</sup>	50.3 ± 2.9	50.2 ± 2.5	0.83
Head diameter (mm) <sup>*†</sup>	32.7 ± 1.8	31.9 ± 2.1	<b>0.005</b>
Number of fixation screws <sup>*†</sup>	0.03 ± 0.2	0.01 ± 0.1	0.88
Cup inclination (degrees) <sup>**†</sup>	37.9 ± 4.6	38.4 ± 4.0	0.13
Cup anteversion (degrees) <sup>*†</sup>	18.5 ± 5.3	17.3 ± 5.3	0.15
Surgery time (min) <sup>*†</sup>	88.1 ± 25.9	82.0 ± 17.7	0.16

<sup>\*</sup>Values are presented as the mean ± SD

<sup>\*\*</sup>Values are presented as the mean ± SD (range)

<sup>†</sup> Mann-Whitney test

<sup>\*\*†</sup> Unpaired t-test

<sup>‡</sup> Pearson's chi-squared test

Statistically significant p-values are presented in bold

**Table 2** Comparison of the JOA score between the highly porous and HA porous groups

JOA score	Highly porous group	HA porous group	p-value
Preoperative	51.6 ± 13.3	50.5 ± 13.7	0.38
Follow-up, 1 year	93.5 ± 5.7	92.6 ± 6.8	0.62
2 years	93.7 ± 5.3	93.5 ± 6.3	0.89
5 years	94.2 ± 6.3	92.3 ± 7.1	0.07

All values are presented as the mean ± SD

The variables were evaluated using the Mann-Whitney U test

porous cups in the same cup system. Our findings indicate that the highly porous cup provided satisfactory clinical outcomes despite a higher incidence of RLLs in the early postoperative period. These RLLs gradually disappeared after 5 years postoperatively, indicating successful long-term osseointegration.

Tamaki et al. reported the short-term outcomes of the G7 OsseoTi highly porous cup compared with the Trident HA-coated porous cup (Stryker, Mahwah, NJ, USA) [15]. Notably, both groups exhibited excellent clinical outcomes; however, RLLs were observed exclusively in the highly porous OsseoTi cup group at rates of up to 22.8% at 24 months postoperatively, without any cases requiring revision surgery. This finding is consistent with our study, which further extended the follow-up period and confirmed that these RLLs tend to disappear after 5 years postoperatively, indicating stable osseointegration. By focusing on the same G7 cup system, this study

provides important information regarding the long-term reliability of the highly porous processing of G7 OsseoTi.

The mechanisms underlying our findings are likely multifactorial. For example, Carli et al. evaluated the Tritanium primary cup (Stryker) and compared it to the Trident HA-coated porous cup over a 5-year follow-up period [17]. They observed a progressive increase in RLLs only with the Tritanium cup, which was designed to be highly porous, requiring cup revision due to aseptic loosening in 1.8% of cases. Histological examination revealed fibrous fixation with reduced osseointegration in the retrieved Tritanium cups. The highly porous design of the Tritanium cup featured excessive porosity (72.5%) and larger mean pore diameter (546 μm) compared with other highly porous cups. This design employed a deposition process in which pure titanium was applied to a scaffold, creating a porous surface [17]. This technique achieved a high degree of porosity; however, it

**Table 3** Comparison of the initial gap between the highly porous and HA porous groups

Parameter	DeLee zone	Highly porous group (109 hips)	HA porous group (89 hips)	p-value
Initial gap (hips)	One or more zones	56 (51%)	46 (52%)	0.97
	1 zone	18 (17%)	8 (9%)	0.12
	2 zone	43 (39%)	39 (44%)	0.54
	3 zone	4 (4%)	5 (6%)	0.51
Follow-up, 1 year	One or more zones	13 (12%)	8 (9%)	0.50
	1 zone	6 (6%)	3 (3%)	0.47
	2 zone	7 (6%)	4 (4%)	0.56
	3 zone	0 (0%)	1 (1%)	0.27
2 years	One or more zones	4 (4%)	2 (2%)	0.56
	1 zone	2 (2%)	1 (1%)	0.68
	2 zone	2 (2%)	0 (0%)	0.20
	3 zone	0 (0%)	1 (1%)	0.27
5 years	One or more zones	1 (1%)	1 (1%)	0.89
	1 zone	1 (1%)	0 (0%)	0.37
	2 zone	0 (0%)	0 (0%)	1.0
	3 zone	0 (0%)	1 (1%)	0.27

The variables were evaluated using Pearson's chi-squared test

**Fig. 1** Incidence of radiolucent lines in highly porous and HA porous groups at 1 year, 2 years, and 5 years postoperatively

introduced structural randomness and variability in pore size and distribution. These factors may contribute to a lower elastic modulus, which induces suboptimal osseointegration or micromotion, finally leading to aseptic loosening. In contrast, the OsseoTi cup used in this study demonstrated a highly controlled and uniform porous surface. The design incorporated 70% porosity and a mean pore diameter of 475  $\mu\text{m}$  through an advanced 3D printing technique called Electron Beam Melting [18]. These factors in the OsseoTi cup may contribute to stable

osseointegration beyond the initial RLL phase. These findings indicate the critical role of the production process for porous surfaces and structural design, including optimized porosity and pore diameter, in achieving effective bone ingrowth. Our results suggest that both surface designs are viable for primary THA. However, we believe that whenever new surface technologies are introduced, such as highly porous coatings designed to mimic human cancellous bone and promote early osseointegration, their presumed clinical advantages must be critically

**Table 4** Comparison of the radiolucent lines between the highly porous and HA porous groups

Follow-up	DeLee zone	Radiolucent lines		p-value
		Highly porous group	HA porous group	
1 year	One or more zones	25 (23%)	2 (2%)	< 0.0001
	1 zone	10 (9%)	1 (1%)	<b>0.014</b>
	2 zone	4 (4%)	0 (0%)	0.068
	3 zone	20 (18%)	1 (1%)	< 0.0001
2 years	One or more zones	21 (19%)	1 (1%)	< 0.0001
	1 zone	9 (8%)	1 (1%)	<b>0.023</b>
	2 zone	4 (4%)	0 (0%)	0.068
	3 zone	17 (16%)	0 (0%)	< 0.0001
5 years	One or more zones	5 (5%)	0 (0%)	<b>0.042</b>
	1 zone	3 (3%)	0 (0%)	0.12
	2 zone	0 (0%)	0 (0%)	1.0
	3 zone	2 (2%)	0 (0%)	0.2

The variables were evaluated using Pearson's chi-squared test

Statistically significant p-values are presented in bold text

**Table 5** Comparison of postoperative total migration between the highly porous and HA porous groups

Follow-up	Total migration (mm)		p-value
	Highly porous group	HA porous group	
1 year*	1.12 ± 0.51	1.20 ± 0.66	0.63
2 years*	1.60 ± 0.85	1.65 ± 0.79	0.82
5 years**	1.94 ± 1.3	2.10 ± 1.2	0.53

All values are presented as the mean ± SD

\* The p-value was evaluated using the unpaired t-test

\*\* The p-value was evaluated using the Mann-Whitney U test

assessed through long-term clinical follow-up to confirm whether they are truly achieved.

This study has some limitations. First, this was a single-center retrospective analysis conducted in an academic hospital, raising the potential for selection bias. The G7 PPS BoneMaster cup (HA porous group) had a slightly longer mean follow-up period due to earlier market availability; however, other demographic data were largely comparable between both groups. Second, we could not evaluate the effects of screw fixation as 98% of all patients in our study did not use screws. However, we thought that it had minimal influence on the outcomes. Third, the femoral components were not included in the analysis. Variations in stem design and alignment might influence the stress distribution of the acetabular cup. However, 99% of the cases in this study utilized the same cementless stem (Taperloc complete microplasty stem; Zimmer Biomet). No periprosthetic fractures were observed around stems during the observation period. Fourth, the timing of radiographic follow-up was not strictly standardized because of the retrospective design of the study. Radiographic data were collected for 2–3 years postoperatively but were grouped as 2-year evaluations, which might have influenced our results. Compared with the findings of Tamaki et al. [15], our study demonstrated a more pronounced reduction in RLLs in the highly porous group between 1 and 2 years postoperatively. We believe

that in the highly porous group, RLLs begin to decrease between 2 and 3 years postoperatively as osseointegration progresses. Therefore, further studies are needed to determine the exact timing of RLL reduction. Fifth, although the observed cup migration values at 5 years, 1.94 mm in the highly porous group and 2.10 mm in the conventional porous group, might appear relatively large, we believe they indicate stable cup fixation. Wyss et al. reported that a gradual decrease in cup migration over time was a critical indicator of successful results using EBRA-based analyses [19]. In our study, both groups demonstrated a consistent reduction in migration over time, suggesting stable cup fixation. Moreover, although EBRA utilizes a comparability algorithm to exclude radiographs with substantially different pelvic tilts or rotations, subtle changes in pelvic tilt over mid-term follow-up might still influence measurement accuracy. Finally, our data was based on a mid-term follow-up. As follow-ups beyond 10 years have not been conducted, further studies with longer follow-up periods are necessary to elucidate the impact of highly porous surfaces.

## Conclusion

The highly porous surface processing in cementless cups was associated with a higher incidence of early RLL formation compared with conventional HA porous coating. However, this does not adversely affect mid-term clinical

outcomes or implant stability. Both surface-processing techniques can provide reliable fixation and excellent clinical outcomes.

#### Abbreviations

HA	Hydroxyapatite
THA	Total hip arthroplasty
RLL	Radiolucent line
EBRA	Einzel-Bild-Röntgen Analysis
JOA	Japanese Orthopedic Association
3D	Three-dimensional
BMI	Body mass index
AP	Anteroposterior
PPS	Porous plasma spray

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#### Author contributions

TT, HK, and JT contributed substantially to the conception of the study. TO contributed to the statistical analysis of the results. KM, MH, RT, RS supervised the study. All authors contributed to the manuscript revision and approved the final version of the manuscript for publication.

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#### Data availability

The data sets used in this study are available from the corresponding author upon request.

#### Declarations

##### Ethical approval and consent to participate

All procedures were conducted in accordance with the principles of the Declaration of Helsinki. The Ethics Committee of the Institute of Science Tokyo, Tokyo, Japan, approved this study. Since participant data was anonymized and because of the voluntary nature of the study, we opted out of the need for informed consent for this study. Written consent to participate was not required for this study design.

##### Consent for publication

Not applicable.

##### Competing interests

The authors declare no competing interests.

##### Clinical trial number

Not applicable.

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